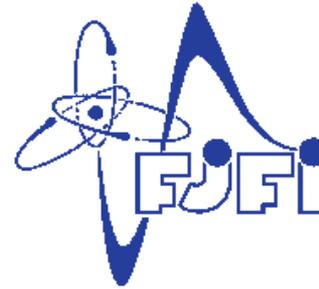
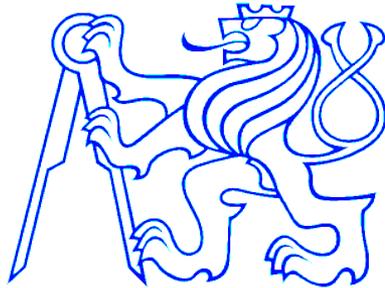


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**Faculty of Nuclear Sciences and Physical Engineering**

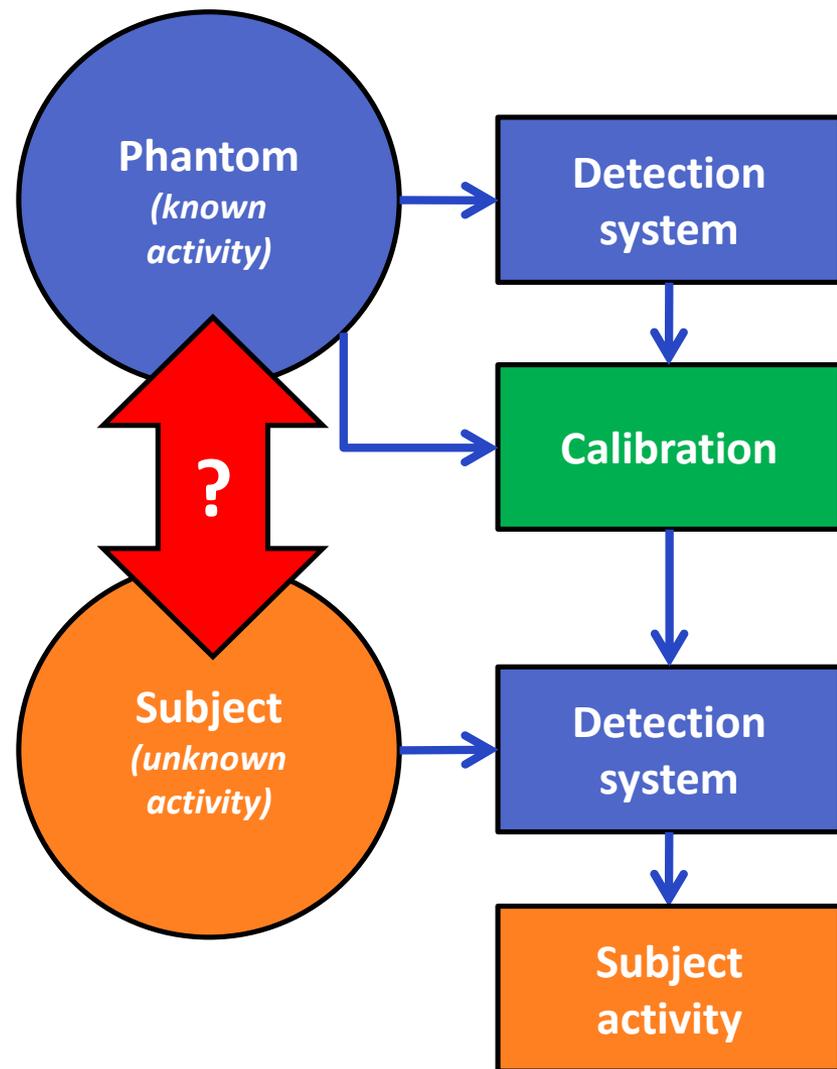


**INFLUENCE OF HEAD SHAPE ON  
MEASURED ACTIVITY  
OF ACTINIDES**

**Tomas Vrba**

# GENERAL CONCEPT OF IN-VIVO MEASUREMENT IN INTERNAL DOSIMETRY

- advantages
  - non destructive
  - relatively fast
  - subject actual activity retention
- disadvantages
  - subject variability
  - activity distribution in subject
  - not applicable for all radionuclides

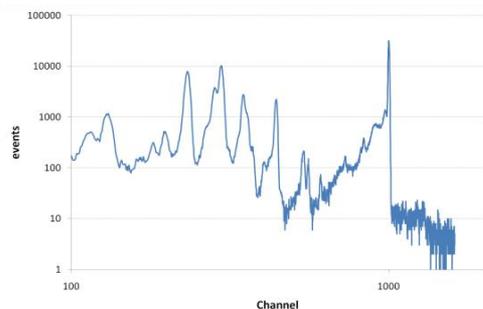


# ACTINIDES ACTIVITY ASSESSMENT – IN VIVO SKULL MEASUREMENT

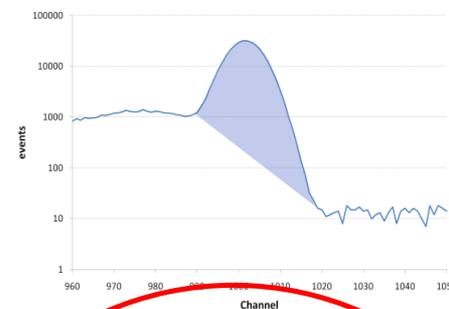
1. skull measurement



2. measured spectra



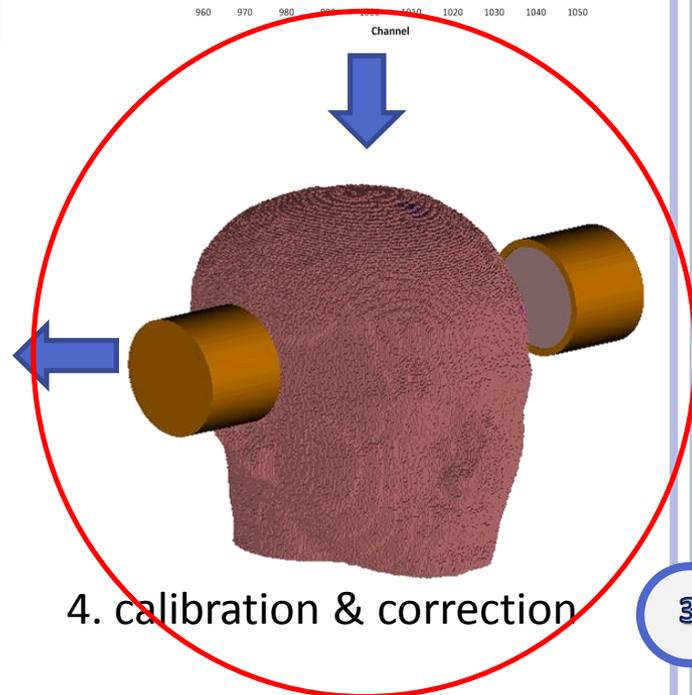
3. net-peak area



6. skeleton activity



5. skull activity

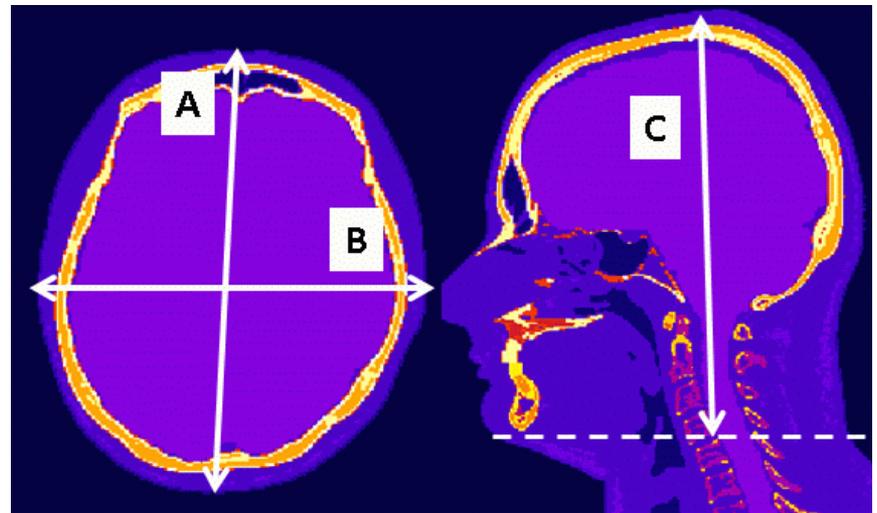


4. calibration & correction

# HOW SKULL SIZE INFLUENCE MEASUREMENT ?

- strength of the effect deepens on detector(s) size and measurement geometry
- head mean radius R
  - measure of the head size

$$R = \frac{A + B + C}{6}$$



- difference in efficiency between minimal and maximal head size about factor 2
  - (Radiat Prot Dosimetry. 2007;127(1-4):201-4)

# HEAD PHANTOMS FOR MC

Phantom	Voxel side (mm)			Diameters (cm)			R (cm)	number of voxels
	x	y	z	A	B	C		
ICRP female <sup>1)</sup>	1.78	1.78	4.84	20.47	14.86	21.30	9.44	715950
ICRP male <sup>1)</sup>	2.14	2.14	8.00	21.08	16.44	22.40	9.98	399156
Linda <sup>2)</sup>	1.00	1.00	1.00	18.70	16.00	21.70	9.40	11175868
<b>Linda simple</b>	2.00	2.00	2.00	18.70	16.00	21.70	9.40	1241550
<b>CIPIC mean head</b>	<b>Not applicable</b>			<b>19.96</b>	<b>14.49</b>	<b>21.46</b>	<b>9.31</b>	

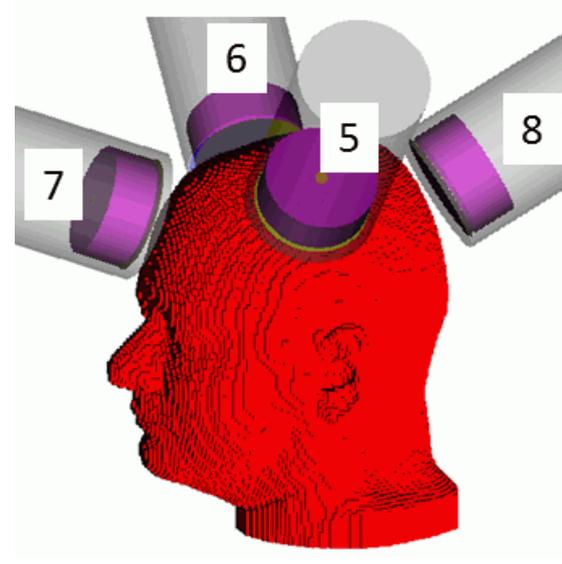
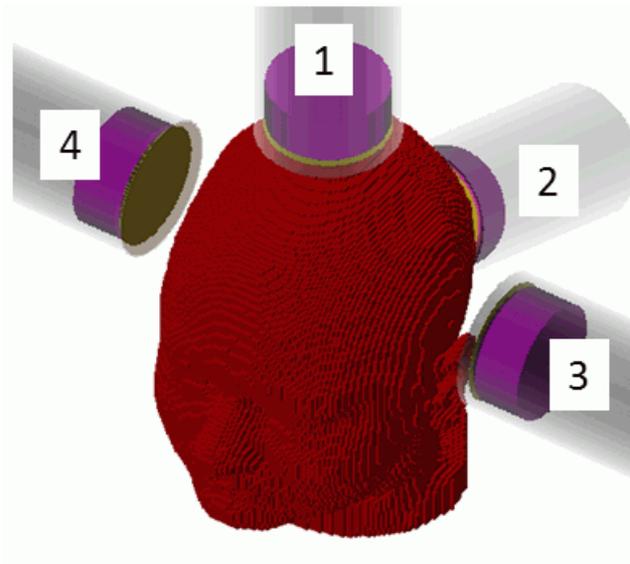
- 1) ICRP reference phantom models (ICRP Recommendation 110)
- 2) woman head phantom (Radiat Prot Dosimetry. 2007;127(1-4):201-4.)

# TYPICAL DETECTORS

- High Purity Germanium (HPGe)
  - different sizes (up to 8 cm in diameter)

Detector property	Canberra (GL3825R)	Ortec (LX-70450-30CW)	detector at NRPI
diameter (mm)	70	70	69.8
depth (mm)	25	30	30.5
window thickness (mm)	0.6	0.6	0.6
FWHM @ 5.9 keV (eV)	475	450	n/a
FWHM @ 122 keV (eV)	750	725	730
crystal to window (mm)	5	4	4

# DETECTOR POSITIONS



Position no.	distance to head (cm)	description
1	1	above skull circa 1-2 cm posteriorly from Bergma
2	1	pointing bottom part of occipital bone
3	3	left temporal bone
4	3	right temporal bone
5	1	between frontal and left parietal bone , angle 52°
6	1	between frontal and right parietal bone, angle -52°
7	1	median part of the frontal bone
8	1	between parietal bones above occipital bone

# PHANTOM SHAPE MODIFICATION

- phantom split to the bone, air, soft tissue subsets
- resizing of three subsets
  - uncorrelated in all three dimensions
  - discrete steps (0.8 - 0.9 - 0.95 - 1 - 1.05 - 1.1 - 1.2)
  - covers ~ 95% percentile of the human skull sizes
  - thickness of the covering tissue kept constant

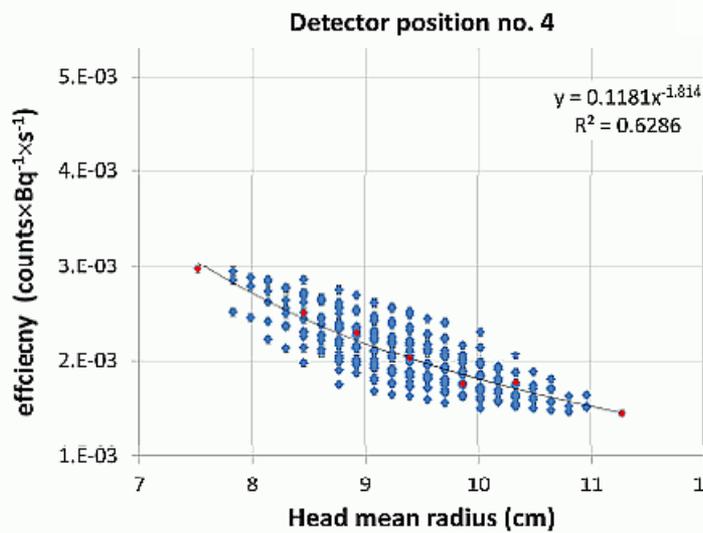
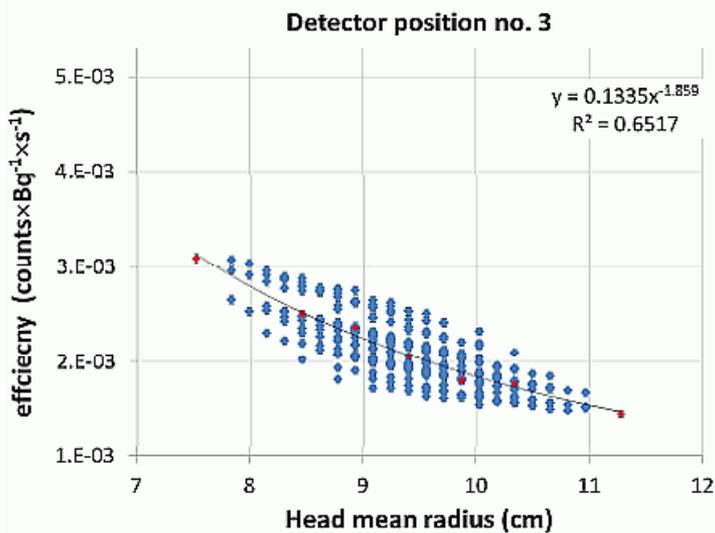
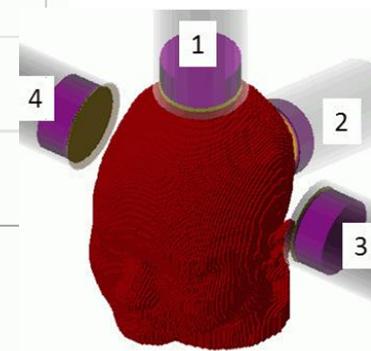
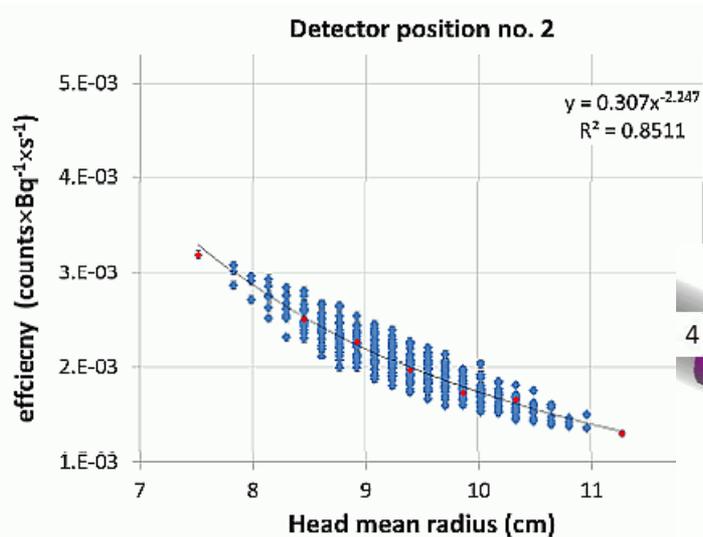
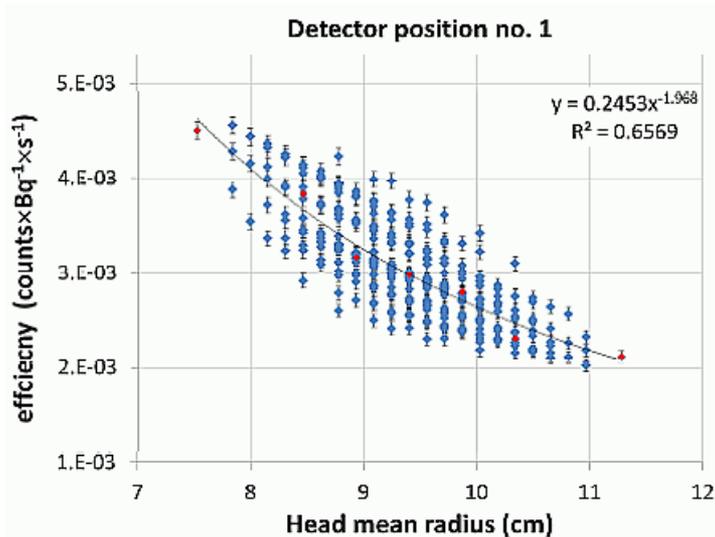


- merging importance (bone > air > soft tissue)
- detector positions adjusted to the new head dimensions

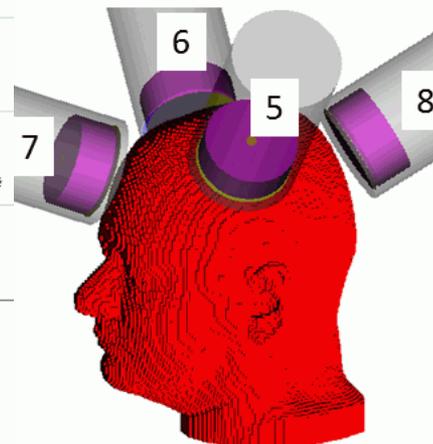
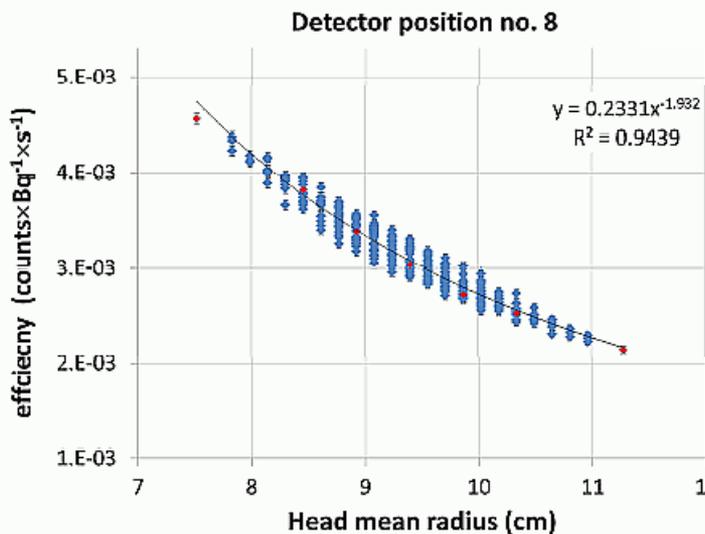
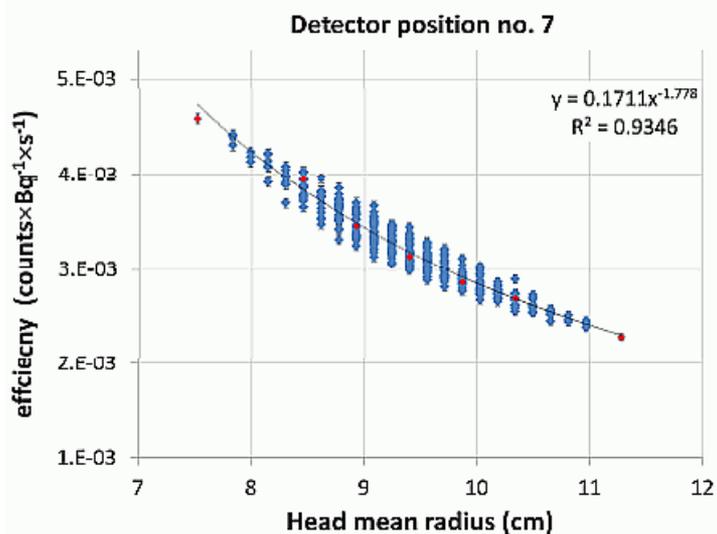
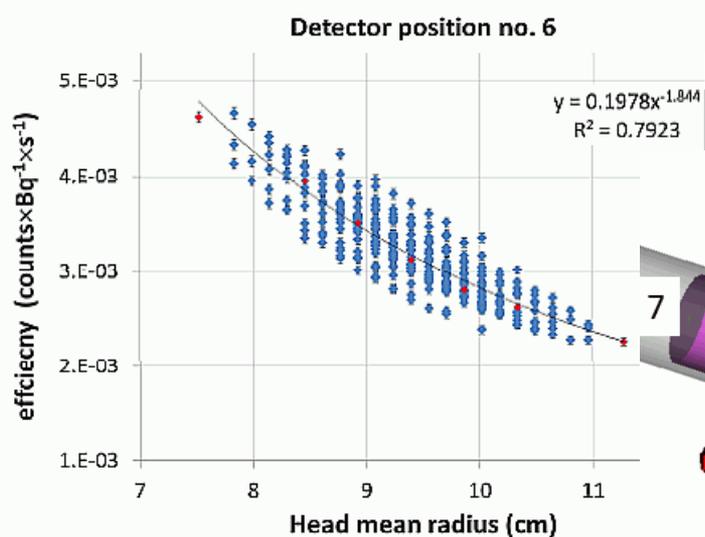
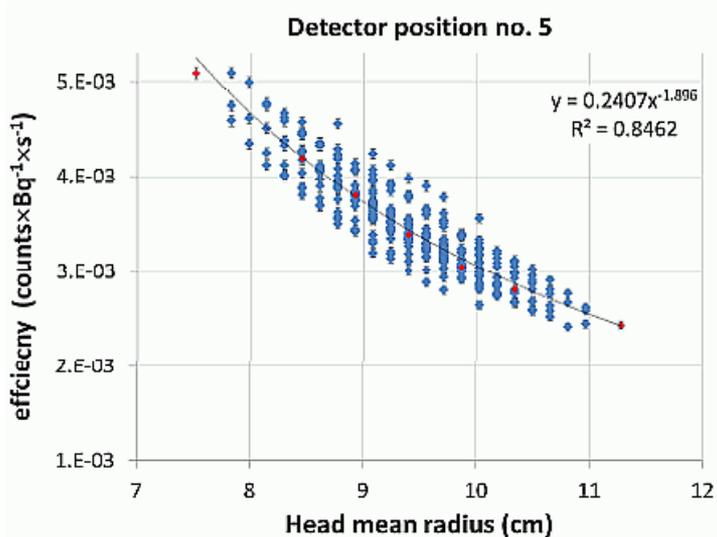
# SIMULATIONS

- MCNPX 2.6, default transport parameters, no GEB
- only photons with  $E = 59.54 \text{ keV}$  ( $^{241}\text{Am}$ )
- homogenous distribution in bone volume
- tally F8 from 55 to 65 keV with 0.5 keV bins
- energy cut-off for non detector cells (ELPT) at 57 keV
  - speedup calculations about factor 2
  - does not affect tally results
- statistical relative standard deviation @ 59.54 bin  $< 0.75 \%$
- 686 simulations

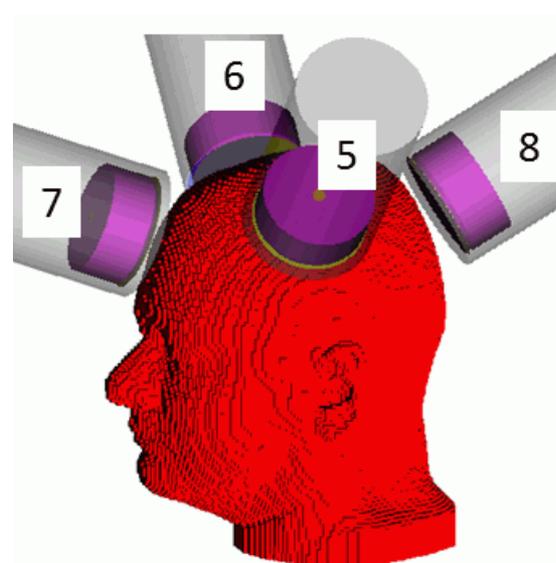
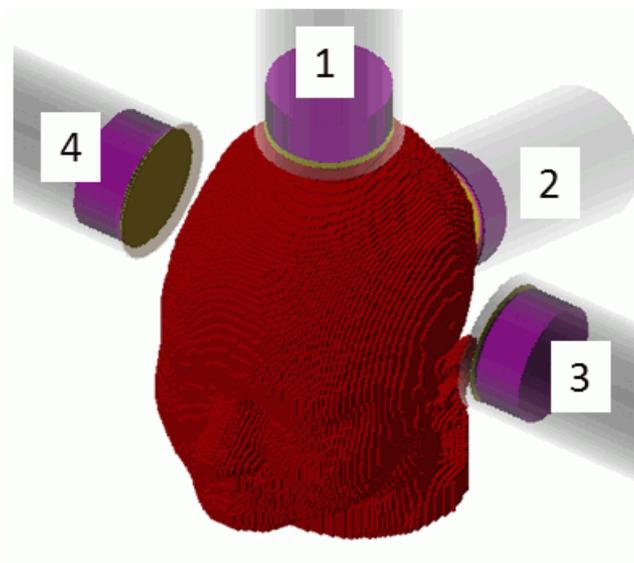
# RESULTS I.



# RESULTS II.



# RESULTS SUMMARY



Parameter	Detector position							
	1	2	3	4	5	6	7	8
Minimal efficiency <sup>a</sup>	2.0E-03	1.3E-03	1.5E-03	1.5E-03	2.4E-03	2.3E-03	2.3E-03	2.1E-03
Maximal efficiency <sup>a</sup>	4.6E-03	3.2E-03	3.1E-03	3.0E-03	5.1E-03	4.7E-03	4.6E-03	4.6E-03
Relative standard deviation due to head shape (%)	10.5	7.0	10.1	10.2	6.0	7.0	3.5	3.5

<sup>a</sup> efficiency in counts×Bq<sup>-1</sup>×s<sup>-1</sup>

## CONCLUSION AND PROSPECT

- estimated uncertainty of detection efficiency due to head shape between 3.5 – 10.5 %
  - less sensitive positions is for median part of the frontal bone and between parietal bones above occipital bone
  - comparable with detector positioning error ( $\sim 12\%$ )
- limitations of presented results
  - uncorrelated head dimensions
    - there is significant correlation between A and B
  - voxel resizing inaccuracy (sub-voxel changes)
- prospect and possible improvement
  - introduce sampling distribution for A, B, C with correlation
  - use NURB phantoms or original Linda phantom
  - integrate it to the total uncertainty of the measurement

# THANK YOU FOR YOUR ATTENTION.

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# BONUS – SKULL PHANTOM COMPARISON

